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# Targeted alpha therapy in vivo: direct evidence for single cancer cell kill using $^{149}\text{Tb}$ -rituximab

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**Abstract.** This study demonstrates high-efficiency sterilisation of single cancer cells in a SCID mouse model of leukaemia using rituximab, a monoclonal antibody that targets CD20, labelled with terbium-149, an alpha-emitting radionuclide. Radio-immunotherapy with 5.5 MBq labelled antibody conjugate (1.11 GBq/mg) 2 days after an intravenous graft of  $5 \cdot 10^6$  Daudi cells resulted in tumour-free survival for >120 days in 89% of treated animals. In contrast, all control mice (no treatment or treated with 5 or 300  $\mu\text{g}$  unlabelled rituximab) developed lymphoma disease. At the end of the study period,  $28.4\% \pm 4\%$  of the long-lived daughter activity remained in the body, of which 91.1% was located in bone tissue and 6.3% in the liver. A relatively high daughter radioactivity concentration was found in the spleen ( $12\% \pm 2\%/g$ ), suggesting that the killed cancer cells are mainly eliminated through the spleen. This promising preliminary in vivo study suggests that targeted alpha therapy with  $^{149}\text{Tb}$  is worthy of consideration as a new-generation radio-immunotherapeutic approach.

**Keywords:** Alpha particle-emitting radionuclides – Terbium-149 – Radio-immunotherapy – Rituximab – Leukaemia

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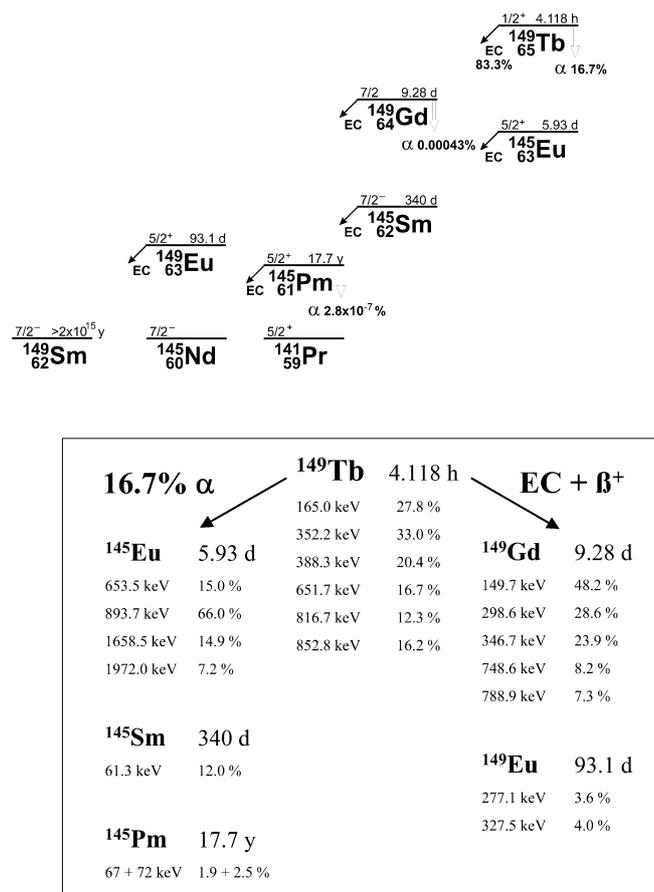
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## Introduction

Single cancer cells in circulation and small cancer cell clusters can be effectively targeted with radio-immunoconjugates that specifically bind to the cells and deliver the required dose. Alpha-emitting radionuclides may be of great advantage in this kind of therapy because of their higher linear energy transfer (LET) value and, consequently, the shorter penetration track compared to  $\beta^-$ - and  $\gamma$ -radiation [1]. It has been shown that only a very few alpha-hits are sufficient to kill a cell [2], and the short range of the alpha particles increases the safety profile of alpha-emitters because non-specific irradiation of normal tissue (or plasma) around the target cells is greatly reduced or absent [3]. Additionally, since single cancer cells in circulation are immediately accessible to the injected (i.v.) radio-immunoconjugate, the shorter half-lives of a few alpha-emitting radionuclides may be advantageous [4]. Only a small number of alpha-emitting radionuclides fulfill the requirements for this specific nuclear medical application:  $^{225}\text{Fm}$ ,  $^{225}\text{Ac}$ ,  $^{224}\text{Ra}$ ,  $^{223}\text{Ra}$ ,  $^{213}\text{Bi}$ ,  $^{212}\text{Bi}$ ,  $^{211}\text{At}$  and  $^{149}\text{Tb}$ . Especially  $^{213}\text{Bi}$  and  $^{211}\text{At}$  have proven to be very promising candidates, because of the availability ( $^{225}\text{Ac}/^{213}\text{Bi}$  generator) and the convenient half-life of 7.2 h ( $^{211}\text{At}$ ) (for example see refs. [5, 6]).

Today, new approaches in conjugation with chelating ligands allow the stable labelling of macromolecules (such as monoclonal antibodies) or peptides with metallic radionuclides. The first clinical proof-of-principle of targeted alpha therapy was observed using the HuM195 antibody labelled with the short-lived (46 min)  $^{213}\text{Bi}$  radionuclide [7], which is a daughter product in the decay chain of  $^{225}\text{Ac}$  (10 days). The mother nuclide,  $^{225}\text{Ac}$ , is itself considered a candidate for targeted alpha therapy (TAT), and corresponding studies are ongoing [3, 8]. A



**Fig. 1.** Simplified decay scheme of  $^{149}\text{Tb}$  and the list of the most relevant gamma transitions (adopted from [17]). Note that the decay of the  $^{149}\text{Tb}$  itself as well as the first daughter products is accompanied by relatively intense gamma emission, while the longer-lived daughter products of the second and third generations show very little gamma contribution

potential drawback with use of  $^{225}\text{Ac}$  is the possibility that the short-lived alpha-emitting daughter nuclides in the decay chain will escape from the place of origin, leading to uncontrolled deposition of the radiation dose throughout the body.

The partial alpha-emitting nuclide  $^{149}\text{Tb}$  ( $T_{1/2}=4.118$  h,  $E_{\alpha}=3.967$  MeV; range in tissue =28  $\mu\text{m}$ ), which belongs to the group of rare earth elements, has been proposed as a promising alpha-emitter for TAT [4, 9, 10, 11]. Its chemical behaviour is very close to that of yttrium or lutetium, whose isotopes  $^{90}\text{Y}$  and  $^{177}\text{Lu}$  are currently the most predominant metallic radionuclides used in clinical radio-immunotherapy (RIT) [12]. Thus, existing approaches for labelling of chelated bioconjugates with these metallic radionuclides, as well as  $^{166}\text{Ho}$ ,  $^{153}\text{Sm}$ ,  $^{213}\text{Bi}$  or  $^{225}\text{Ac}$ , can be directly applied to  $^{149}\text{Tb}$ . Previous in vitro studies have revealed certain advantages of  $^{149}\text{Tb}$  over  $^{213}\text{Bi}$  for treating single cells [13]. These advantages, which relate to the lower energy and higher LET of alpha particles emitted by  $^{149}\text{Tb}$ , partially

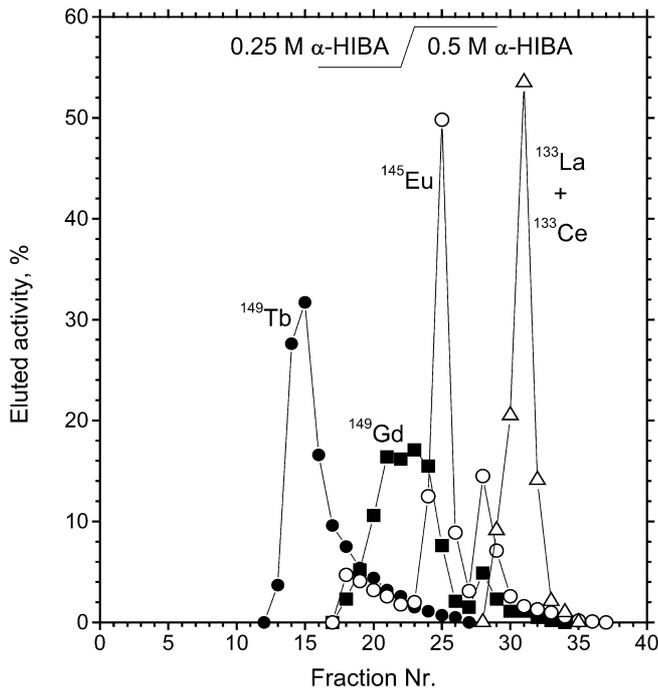
compensate for its lower alpha branching (17%, Fig. 1) [13, 14]. The longer half-life of  $^{149}\text{Tb}$  (4.12 h) compared with  $^{213}\text{Bi}$  (46 min) represents a clear advantage, both at the level of bioconjugate preparation and for administration to patients for tumour cell targeting. On the other hand, the fate of long-lived daughter products that appear during the decay of  $^{149}\text{Tb}$  would need to be considered carefully in the dosimetry (Fig. 1).

In this paper we describe the first in vivo survival study using a  $^{149}\text{Tb}$ -based TAT approach in SCID (severe combined immuno-deficient) mice. SCID mice, being deficient in T and B cell immune defence, easily develop tumour masses after injection of cancer cells. Daudi cells, which are derived from a human Burkitt lymphoma, are one of several cell lines that can rapidly colonise these mice. Depending on the injection route, different tumour types can develop. As few as 100 injected (i.v.) Daudi cells are sufficient to kill SCID mice due to tumour development [15]. Since Daudi cells express a high number of CD20 antigens, rituximab can target Daudi cells with high specificity. Thus, an early stage of this model, within 3 days of i.v. xenograft, before the formation of manifested tumour nodes, provides an ideal system to study the proposed advantages of  $^{149}\text{Tb}$ -based TAT.

The primary aim of this work was to examine the efficacy of  $^{149}\text{Tb}$ -labelled rituximab to specifically kill circulating single cancer cells or small cell clusters in vivo. SCID mice following i.v. xenograft with Daudi cells represent a perfect model for leukaemia [16]. Our experimental model involves TAT intervention within 3 days of i.v. xenograft, and hence before the formation of manifested tumour nodes, which we did not intend to target in this study. According to our experimental hypothesis, mice xenotransplanted with a lethal number of Daudi cells will survive provided that a sufficient dose of  $^{149}\text{Tb}$  has been delivered via rituximab to all tumour cells. Secondly, we aimed to obtain information about the behaviour of the daughter products generally formed in the radioactive decay chain. The 17% alpha decay mode of the  $^{149}\text{Tb}$  generates an isobar chain with the mass number  $A=145$  with  $^{145}\text{Eu}$  ( $T_{1/2}=5.93$  days),  $^{145}\text{Sm}$  ( $T_{1/2}=340$  days) and  $^{145}\text{Pm}$  ( $T_{1/2}=17.7$  years). The EC-process decay chain of  $^{149}\text{Tb}$  forms the stable  $^{149}\text{Sm}$  passing the  $^{149}\text{Gd}$  ( $T_{1/2}=9.28$  days) and the  $^{149}\text{Eu}$  ( $T_{1/2}=93.1$  days) ([17], Fig. 1). Most of these isotopes are easily detectable using high-resolution gamma spectroscopic techniques (Fig. 1). In particular, we expected that differences in daughter isotope behaviour induced by the different decay modes (alpha versus EC) would be apparent.

## Materials and methods

**Cell line.** Daudi cells (ATCC Nr. CCL-213) were used to simulate a leukaemia model in mice. The cells were cultured in RPMI 1640 medium supplemented with 10% heat-inactivated fetal calf serum and 0.5% penicillin (10,000 U/ml)/streptomycin (10 mg/ml) (Sig-



**Fig. 2.** Separation of the A=149 isobars obtained in the on-line isotope separation process at ISOLDE by using cation exchange chromatography. Column: Aminex A 5 in  $\text{NH}_4^+$  form,  $3 \times 60 \text{ mm}^2$ , eluent:  $\alpha$ -HIBA, elution speed:  $100 \mu\text{l}/\text{min}$  (one drop =  $35 \mu\text{l}$  = one fraction). The isotopic content of each fraction has been determined by high-resolution gamma ray spectrometry

ma-Aldrich). The cell suspension to be injected into mice was prepared by centrifuging the culture for 3 min at 1,200 rpm, washing with PBS and re-suspending in PBS at  $2.5 \cdot 10^7$  cells per ml.

**Antibody conjugate.** Rituximab antibody (Rituxan; IDEC Pharmaceuticals, San Diego, and Genentech Inc, San Francisco) is a chimeric version of anti CD-20 monoclonal antibody consisting of human  $\text{IgG}_1$  constant domains and murine variable domains. The rituximab antibody conjugated with SCN-CHX-A-DTPA (2-(4-isothiocyanatobenzyl)-cyclohexyl-diethylenetriamine penta-acetic acid), used in this study, was kindly provided by Dr. D.A. Scheinberg (Memorial Sloan Kettering Cancer Center, New York).

**Radionuclide.** The  $^{149}\text{Tb}$  was produced using the on-line isotope separator facility ISOLDE at CERN (Geneva, Switzerland) [18, 19]. A tantalum-foil target ( $120 \text{ g}/\text{cm}^2$ ) was irradiated with 1.0- or 1.4-GeV protons delivered from the CERN PS-Booster accelerator. The radio-lanthanides generated in the spallation process are released from the target material, which is kept at about  $2,200^\circ\text{C}$ , ionised by surface ionisation and accelerated to 60 keV. From the obtained radioactive ion beams, the A=149 isobars ( $^{149}\text{Dy}$ ,  $^{149}\text{Tb}$  and molecular ions  $^{133}\text{CeO}^+$  and  $^{133}\text{LaO}^+$ ) were implanted (60 keV) and thus collected in thin layers of  $\text{KNO}_3$  ( $10 \text{ mg}/\text{cm}^2$ ) on aluminium backings. The  $^{149}\text{Tb}$  was separated from its daughters ( $^{149}\text{Gd}$  and  $^{145}\text{Eu}$ ) and the pseudo-isobars  $^{133}\text{Ce}$  and  $^{133}\text{La}$  by cation exchange chromatography using Aminex A5 resin and  $\alpha$ -hydroxyisobutyric acid as eluent. A typical elution chromatogram is presented in Fig. 2. The  $^{149}\text{Tb}$  fraction ( $150\text{--}200 \mu\text{l}$ ) was evaporated to dryness and re-dissolved in  $50 \mu\text{l}$  of  $100 \text{ mM HCl}$ . The final  $^{149}\text{Tb}$  concentration was  $2 \text{ GBq}/\text{ml}$  ( $54 \text{ mCi}/\text{ml}$ ) at the end of chromatographic separation (EOS).

**Labelling procedure.** From 25 to  $40 \mu\text{l}$  of the  $^{149}\text{Tb}$  solution characterised above was used immediately for the labelling procedure. The pH was adjusted to 5.5 by adding  $60 \mu\text{l}$  of  $3 \text{ M CH}_3\text{COONH}_4$  solution, followed by the addition of  $10 \mu\text{l}$  ( $40 \text{ mg}/\text{ml}$ ) ascorbic acid. After adding  $5 \mu\text{l}$  of a stock solution of the chelated antibody in PBS ( $10 \text{ mg}/\text{ml}$ ), the mixture was incubated for 10 min at room temperature, before dilution to a final volume of 1.0 ml in PBS-1% human serum. The radiochemical purity of the labelled rituximab was determined by instant thin-layer chromatography ( $1.5 \times 15 \text{ cm}$  ITLC-SG strips, Gelman Instrument Company) using  $0.1 \text{ M}$  acetate buffer of pH 6 as a mobile phase and the linear analyser (Berthold). The injection of the radio-immunoconjugate into the mice was performed 1 h after EOS. The in vitro behaviour of the labelled bioconjugate (immunoreactivity, cell binding, cell killing efficiency) has been described in a previous paper [14]. With the same antibody we observed up to 55% cell binding without extrapolation to infinite antigen excess.

**Mice survival studies.** The in vivo studies were performed using 26 female SCID mice (C.B.-17/ICR, Iffa Credo) under the authorisation Nr: GE 31.1.1049/1879/II. The mice, which were 8 weeks old at the start of the experiment and weighed 20 g on average, were kept in sterile, ventilated boxes. Before injecting cells and antibodies, mice were anaesthetised by i.p. (intraperitoneal) injection of 10 ml per kg (typically 0.2 ml) of an anaesthetic (2.4 ml Ketasol 50, 0.8 ml Rompun, 6.8 ml 0.9% NaCl). Each mouse re-

**Table 1.** Summary of the in vivo experiments on SCID mice xenotransplanted with Daudi cells and treated by immunotherapy or radio-immunotherapy with  $^{149}\text{Tb}$ -labelled rituximab

	SCID mice groups			
	Group 1	Group 2	Group 3	Group 4 (control group)
No. of mice per group	6	4	9	6
First i.v. injection	$5 \cdot 10^6$ Daudi cells			
Second i.v. injection 2 days after Daudi cell inoculation	$5 \mu\text{g}$ rituximab	$300 \mu\text{g}$ rituximab	$5 \mu\text{g}$ $^{149}\text{Tb}$ -labelled rituximab (5.55 MBq)	None
Results during follow-up (up to 120 days after the therapy)	17% developed macroscopic tumours, 83% showed paralysis or weight loss	50% developed macroscopic tumours, 50% showed paralysis or weight loss	89% had no pathological changes, 11% had abdominal tumour growth	50% developed macroscopic tumours, 50% showed paralysis or weight loss

ceived  $5 \cdot 10^6$  Daudi cells by injection of 0.2 ml cell suspension in PBS into the tail vein. Two days after xenotransplantation the mice were divided into four groups: the first group received 5  $\mu$ g rituximab in 0.1 ml PBS i.v.; the second group, 300  $\mu$ g rituximab in 0.1 ml PBS i.v.; and the third group, 5.5 MBq  $^{149}\text{Tb}$ -CHX-A-DTPA-rituximab radio-immunoconjugate (5  $\mu$ g labelled rituximab in 0.2 ml, i.v.); the fourth group was left without any treatment. A summary of the *in vivo* study is presented in Table 1. According to the authorised protocol, the mice were surveyed for 120 days: their behaviour was logged each day, their condition was supervised once a week by a veterinarian, and they were weighed three times a week. At the appearance of obvious signs of paralysis, visible tumour masses or a weight loss of >15%, the mice were sacrificed. One mouse was sacrificed shortly after injection (2 h p.i.) and kept deep-frozen for later analysis, in order to act as a reference for later quantification of the daughter radioactivity distribution.

**Retention and daughter radioactivity distribution.** Organ samples were taken from the sacrificed mice and the radioactivity concentration of the long-lived daughter products was determined by using high-resolution gamma spectroscopy (18% HP-Ge detector in combination with the Gamma spectrometer Genie 2000, Canberra). Whole, intact mice, as well as isolated organ samples, were measured. Since the radioactivity content of the samples was essentially very low, long measuring times (between 1 and 24 h) were applied.

**Statistical analysis.** The survival of animals until sacrifice because of disease development or the end of the experiment (no disease development) was compared between the different groups according a Kaplan Meier analysis using the Lee-Desu evaluation of the Unistat 3.0 statistical package (Megalon, Novato CA, USA).

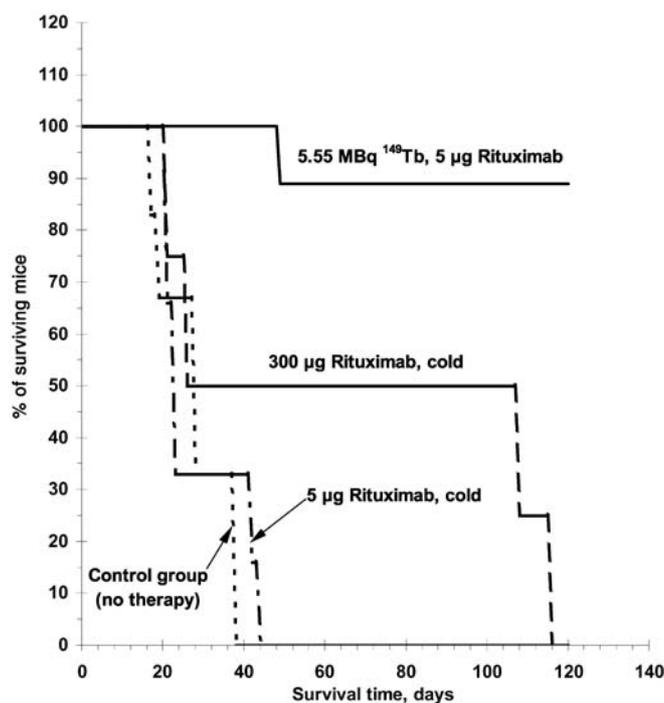
## Results

### Preparation of labelled rituximab

Mass-separated and radiochemically pure  $^{149}\text{Tb}$  was obtained after chromatographic separation of the collected isobars with mass number  $A=149$  at the on-line mass separator facility at CERN (Fig. 2). The overall time needed for the radiochemical separation and the labelling procedure was 1 h. Radiolabelling of the rituximab with this  $^{149}\text{Tb}$ -preparation was almost quantitative (>99%) within 10 min incubation time. The obtained preparation was thus ready for injection without further purification. The radioactivity concentration of the labelled antibody solution was 27.8 MBq/ml (0.75 mCi/ml), while the specific activity was 1.11 GBq/mg (30 mCi/mg) at the moment of injection.

### Survival in a SCID mouse model of leukaemia

We set out to evaluate the efficacy of  $^{149}\text{Tb}$ -based TAT using a SCID mouse model of leukaemia [16]. Our experimental model involved the i.v. xenografting of a lethal number of Daudi cells followed by TAT intervention



**Fig. 3.** Survival graph of SCID mice grafted with  $5 \cdot 10^6$  Daudi cells i.v., followed by different i.v. treatments 2 days after xenotransplantation (for details see text)

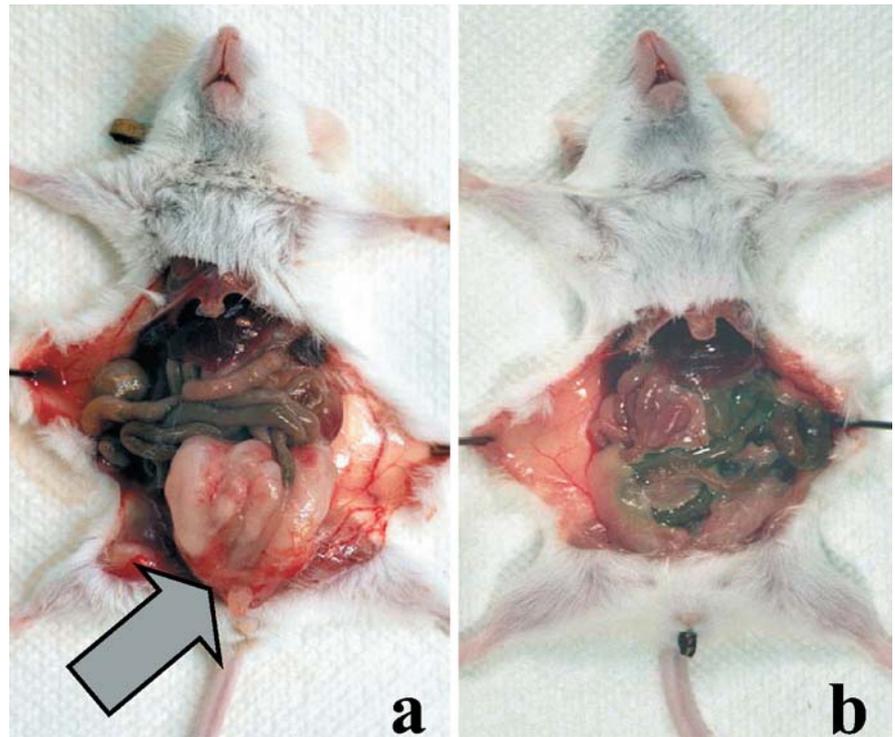
at a time point when most of the Daudi cells would be expected to remain in circulation, and before the appearance of manifested tumours, which we did not intend to target in this study. Survival data over a period of 4 months for treated mice and controls are shown in Fig. 3. All mice in the untreated control group developed clear signs of Burkitt lymphoma and were consequently sacrificed within 37 days. Fifty percent of them developed visible macroscopic tumours while the others were sacrificed when they showed clear signs of paralysis or a weight loss >15% of the initial body weight (Table 1).

The injection of a single, low dose of rituximab (5  $\mu$ g/animal) did not show any therapeutic effect, and all mice in this group had to be sacrificed within 43 days. As can be seen from Fig. 3, the survival curves of this group and the control group (untreated mice) are almost identical. Of the mice in this group, 83% expressed obvious signs of paralysis or weight loss of >3 g, while 17% developed visible macroscopic tumour masses.

A different survival pattern was observed after treatment with a high dose of rituximab (300  $\mu$ g per animal, corresponding to 15 mg/kg). Although a single dose of 15 mg/kg rituximab significantly increased the life expectancy—50% of mice in this group survived 100 days—ultimately, tumours developed in all animals (an example is shown in Fig. 4a) before the end of the observation period.

In contrast, the mice treated with the radioactive  $^{149}\text{Tb}$ -CHX-DTPA-rituximab (5  $\mu$ g rituximab per animal) were almost completely protected over the entire

**Fig. 4 a.** Dissected mouse from the control group that received 300 µg rituximab, with clearly visible large tumour in the abdomen (*arrow*). **b** Dissected mouse grafted with Daudi cells and treated by  $^{149}\text{Tb}$ -CHX-A-DTPA-rituximab after 120 days, without any visible signs of disease



**Table 2.** Biodistribution of  $^{149}\text{Tb}$ -labelled rituximab in SCID mice 2 h after i.v. injection and of the remaining daughter radioactivity distribution 120 days after injection

Organ	2 h p.i.		120 d p.i.	
	(% i.d./organ)	(%/g tissue)	(% i.d./organ)	(%/g tissue)
Blood	n.a.		<0.01	
Liver	18±3	24±4	1.8±0.3	1.6±0.2
Bone <sup>a</sup>	13±1	9.1±0.7	26±4	13±2
Spleen	1.9±0.2	42±4	0.40±0.06	12±2
Heart	4.7±0.7	41±6	<0.01	
Lung	2.4±0.5	18±4	<0.01	
Kidney <sup>b</sup>	6±1	24±4	0.2±0.03	0.50±0.08
Muscles		<0.2	<0.02	
Bladder <sup>c</sup>	0.12±0.03	3.7±0.9	<0.01	
Body, total	100		28.4±4	

Note that both femurs and both kidneys were combined for the gamma spectroscopic measurements in order to increase the signal to background ratio

n.a., Not done/not assessable

<sup>a</sup> Bone total was calculated as 9 × activity of both femora

<sup>b</sup> Both kidneys were measured together

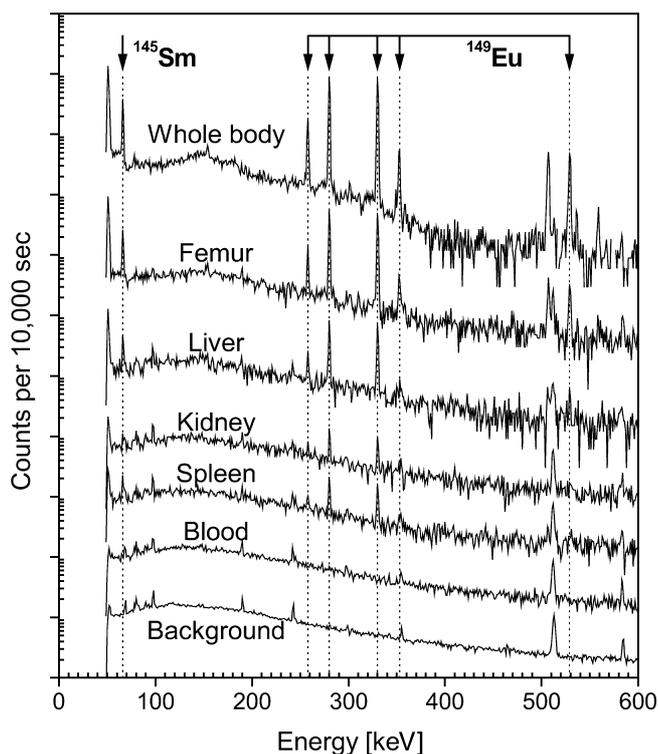
<sup>c</sup> Bladder measured with urine

observation period, with only one mouse in this group being lost after 48 days due to abdominal tumour growth. The remaining eight mice (89%) showed normal behaviour without any signs of disease for 4 months after grafting (Fig. 4b). All of these mice were sacrificed after 120 days and were found to be tumour free at dissection. Thus, a single injection of 5.5 MBq  $^{149}\text{Tb}$ -labelled rituximab (5 µg MoAb), which corresponds to an injected dose of 280 MBq/kg body weight (7.5 mCi/kg), produced long-term survival without evidence of any

disease at 120 days. The survival increase after the RIT compared with all the control groups (no treatment, 5 µg and 300 µg unlabelled rituximab) was highly significant in the statistical Lee-Desu comparisons ( $P < 0.005$ ).

#### *Biodistribution of labelled rituximab and the daughter radionuclides*

In Fig. 5 we present typical gamma spectra of retained activity in organs recorded 120 days after injecting the



**Fig. 5.** Typical gamma spectra of retained daughter radioactivity in organs taken 120 days after injecting the radio-immunoconjugate into the mice

short-lived radio-immunoconjugate. The biodistribution of  $^{149}\text{Tb}$ -CHX-A-DTPA-rituximab radio-immunoconjugate shortly after injection was assessed using a single mouse sacrificed at 2 h. The retention of the long-lived daughter nuclides at 120 days after injection is presented in Table 2. After 2 h, the organs with high blood pool, like the spleen, heart and kidney (42%, 41% and 24% ID/g), showed relatively high radioactivity concentration. High amounts of the radio-immunoconjugate were found in the liver at this time point ( $18\% \pm 3\%$  injected dose), confirming the results of earlier systematic studies [20]. The values in the other organs were relatively low. After 120 days, 71.6% of the primary injected radioactive atoms had been excreted from the mice. The retention of the daughter products was  $28.4\% \pm 4\%$ , of which 91.1% remained in the bone tissue and 6.3% in the liver.

## Discussion

### *Protection of mice treated with labelled rituximab*

Here we show that TAT with rituximab labelled with the high-purity alpha-emitting radio-lanthanide  $^{149}\text{Tb}$  led to almost complete protection of xenografted mice over 4 months without detectable signs of toxicity, under conditions where all animals in the control groups had to be sacrificed during the observation period due to the devel-

opment of tumour diseases. The efficacy of the radionuclide bioconjugate as opposed to the unconjugated tumour targeting antibody alone is underlined by the complete lack of protection in the control group that received 5  $\mu\text{g}$  unlabelled rituximab per animal, and the relatively poor protection afforded by the higher dose unlabelled rituximab group (300  $\mu\text{g}$  per animal). The degree of protection afforded by the  $^{149}\text{Tb}$ -labelled rituximab indicates that TAT with  $^{149}\text{Tb}$  is, on the basis of its efficacy, worthy of further consideration as a novel radio-immunotherapeutic strategy.

### *Biodistribution of label and decay products*

From earlier studies we have learnt that once the lanthanides are trapped in a tissue, like liver or bone, they are fixed quite stably [20, 21]. The blood clearance for free radio-lanthanides or radio-lanthanides injected in solutions containing chelate ligands (citrate, EDTMP, NTA, EDTA, DTPA and others) is fast (half-time <1 h) [21, 22]. The radio-lanthanides are then present mainly in the bone matrix and the liver, with the liver uptake determined by the ionic radius of the lanthanide [21, 22, 23]. In the case of macromolecules (like monoclonal antibodies) the blood clearance is slow (half-time  $\sim$ 1 day) [20]. Thus, most of the  $^{149}\text{Tb}$  will decay while the labelled bioconjugate is in circulation and the free daughter nuclides formed in the radioactive decay would follow the biodistribution known for free radio-lanthanides. The biodistribution found 120 days after treatment corresponds to the distribution patterns known for the free radio-lanthanide: highest daughter nuclide accumulation in bone and liver (91.1% and 6.3% of the retained activity, respectively) [21, 22]. The spleen shows a radioactivity concentration almost as high as bone and significantly higher compared with liver. We interpret this result as evidence that the targeted and killed cancer cells are eliminated mainly through the spleen, where the remaining radioactive daughter atoms are then trapped.

The long-lived daughter products are formed along two main decay processes: the isobar chain with  $A=145$  is generated via the alpha decay mode of the initial  $^{149}\text{Tb}$ , while the isobar chain with  $A=149$  is formed after the EC- or  $\beta^+$ -process. In the case of an alpha decay, the recoil energy of the  $^{145}\text{Eu}$  daughter nuclei (110 keV) exceeds significantly the chemical binding energy. Consequently, the original molecule, the antibody construct, is destroyed and the daughter atom is initially stabilised as free  $\text{Eu}^{3+}$  ion. In the case of the EC-decay mode, the bond rupture is induced due to the Auger electron emission forming free daughter species [24, 25] with 100% efficiency. However, it cannot be assumed that the daughter species escapes from its place of origin; it could eventually be bound to other proteins in the immediate environment. Consequently, one may not necessarily expect identical behaviour from daughter products

**Table 3.** Radioactivity level of long-lived daughter products retained in a patient after injection of 1 GBq  $^{149}\text{Tb}$ -rituximab antibodies, assuming 100% retention of the long-lived daughter products (worst case)

$t_{\text{p.i.}}$	$^{149}\text{Tb}$	$^{149}\text{Gd}$	$^{149}\text{Eu}$	$^{145}\text{Eu}$	$^{145}\text{Sm}$	$^{145}\text{Pm}$
=0	$T_{1/2}=4.12\text{ h}$ 1.0 GBq	9.28 days	93.1 days	5.93 days	340 days	17.7 yrs
2 days	310 kBq	13 MBq	0.2 MBq	3.9 MBq	18 kBq	
5 days		11 MBq	0.4 MBq	2.7 MBq	37 kBq	43 Bq
10 days		7.3 MBq	0.7 MBq	1.5 MBq	57 kBq	86 Bq
100 days		8 kBq	0.7 MBq	41 Bq	70 kBq	0.8 kBq
1 yr			0.1 MBq		41 kBq	2.2 kBq
10 yrs			0		50 Bq	3.1 kBq

The retention was measured to be only 28.4% independent of the decay mode (alpha or EC) (see Table 2); thus the real activity of daughter products would be nearly a factor of 4 smaller. On the other hand, the injection of a  $^{149}\text{Tb}$ -labelled bioconjugate 4 h after

the Tb purification would increase the activity of the daughter product by a factor of 2. In this way the numbers in this table can still be seen as upper limits

generated in the two different pathways: alpha or EC process. Analysis of the gamma spectroscopic data revealed that there was no statistically significant difference in the ratio of retained  $^{145}\text{Sm}$  to  $^{149}\text{Eu}$  in the organs from that predicted by the branching ratio of  $^{149}\text{Tb}$ . Thus, the radioactive decay pathway does not influence the biodistribution or redistribution of the long-lived daughter lanthanides.

#### Extrapolation to clinical application

A preliminary dose estimation for patients injected with 5 GBq  $^{149}\text{Tb}$ -rituximab was performed based on MIRDOSE 3.1 [26]. Assuming total decay of  $^{149}\text{Tb}$ -rituximab in circulation and 100% retention of daughter nuclides in the body with a bone uptake of 91%, the total equivalent dose to the bone marrow as the critical organ would be 540 mSv/5 GBq (108 mSv/GBq) (see also Table 3).  $^{149}\text{Tb}$  itself would contribute 66.7% of the bone marrow radiation dose (45.2% due to the  $\alpha$ -radiation using an  $\alpha$ -radiation weight factor of  $W_R=10$ ) and 21.5% due to its  $\gamma$ - and  $\beta^+$ -radiation) while the daughter nuclides would contribute 33.3% only. The dose contribution from daughter nuclides estimated in this way represents a worst-case estimation (assuming 100% retention), since only 28.4% of the long-lived daughter products were retained in mice 120 days p.i. Thus, injection of a potentially therapeutic activity, 5 GBq  $^{149}\text{Tb}$ -rituximab, in a 70-kg patient, would deliver a bone marrow radiation dose far below the critical level. This preliminary dose estimation is well compatible with considerations presented in the review by McDevitt et al. [8].

For further reduction of the retention of the daughter nuclides one could apply single or multiple injections of chelating ligands like EDTA or DTPA during or shortly after the treatment. This approach is already practiced as a preventive action in treatments with  $^{90}\text{Y}$ - or  $^{177}\text{Lu}$ -DOTATOC [27].

#### Time constraints and availability

Spallation reaction in combination with on-line mass separator technology was used for the production of  $^{149}\text{Tb}$  for this study. The radiochemical separation and purification of the  $^{149}\text{Tb}$  were relatively easy to perform in about 30 min in this specific case, since we started from non-carrier-added preparations. The final  $^{149}\text{Tb}$  preparation was obtained in very high purity and in a small volume, and the labelling of the bioconjugate was fast (10 min) and almost quantitative. The administration of the preparation should be carried out as rapidly as possible after purification of the  $^{149}\text{Tb}$ , since levels of contamination with daughter nuclides will increase with time. For example, application of a fixed dose of the  $^{149}\text{Tb}$ -labelled bioconjugate 4 h after the final purification of the isotope itself (EOS) leads to an increase in the long-lived daughter content by a factor of 2. According to the preliminary dose estimation one could define a shelf-life for the  $^{149}\text{Tb}$ -labelled bioconjugate of about 4–6 h. For a longer delay it would be advisable to repurify the  $^{149}\text{Tb}$  from the accumulated daughter products, a process that could require 30 min.

Several nuclear processes could be used to make this interesting alpha-emitting isotope available on large scale: light particle (p, d, He)-induced reactions on  $^{152}\text{Gd}$  as target material, heavy ion-induced reactions on light lanthanide targets or spallation reaction on Ta as target [19]. Off-line and on-line mass separation process may support a very high isotopic purity [19, 28].

For the time being, only a few centres may be able to make this isotope. On the other hand, all the above-mentioned technologies are well developed and available today. In summary, should  $^{149}\text{Tb}$  continue to show promise in further studies of TAT, then it would be technically feasible to make the isotope available on a large scale and on a routine basis.

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