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Forecasting seizure risk in adults with focal epilepsy: a development and validation study

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21 Research in context

22

23 **Evidence before this study:**

24 We searched the literature on seizure prediction in MEDLINE from January 1, 1946, to June 1,
25 2020, in Embase from January 1, 1974, to June 1, 2020, and in Google Scholar (first 200 relevant
26 references) using comprehensive electronic search strategies combining terms “epilepsy”,
27 “seizures”, “prediction”, “forecasting”, “cycles”, “patterns”, “circadian”, and “multidien”, with
28 no language restrictions. Identified studies used different outcome measures, but most involved
29 analyses of electroencephalography (EEG) to predict seizures minutes in advance, with variable
30 success. A single prospective trial of an implanted device for chronic EEG demonstrated above-
31 chance accuracy of warnings for imminent seizures in 9 out of 15 enrolled subjects. Two studies
32 in independent cohorts of subjects chronically implanted with intracranial electrodes showed
33 that rates of interictal epileptiform activity oscillate in circadian and multiday (multidien) cycles
34 that help determine seizure likelihood. Circadian cycles and seizure diaries were used in three
35 studies to forecast seizures over short horizons, but we found no results on forecasting seizures
36 several days in advance.

37

38 **Added value of this study:**

39 In a large cohort of people with drug-resistant focal epilepsy who had chronic EEG recorded by
40 an approved clinical device, we demonstrate that circadian and multidien cycles can be
41 leveraged to forecast seizures up to three days in advance in some subjects and 24 hours in
42 advance in the majority of subjects. These results highlight the feasibility of seizure forecasting
43 over horizons longer than previously possible.

44

45 **Implications of all the available evidence:**

46 Seizures are not entirely random events. Using cyclical patterns of brain activity to forecast
47 seizures hours to days in advance may enable novel seizure warning systems and prevention
48 strategies. Convergence of findings from multiple independent datasets suggests the
49 generalizability of this approach in people with epilepsy, though this will require direct testing in
50 prospective clinical trials.

51 **Abstract**

52

53 **Background**

54 For people with epilepsy, much suffering stems from the apparent unpredictability of seizures.
55 Recently, converging evidence from studies using chronic electroencephalography (cEEG)
56 revealed that brain activity in epilepsy demonstrates robust cycles, operating over hours
57 (circadian) and days (multidien), which help determine fluctuating seizure risk. We hypothesized
58 that cycles of brain activity can be leveraged to estimate future seizure probability, and we
59 tested the feasibility of forecasting seizures days in advance.

60

61 **Methods**

62 This feasibility study involved retrospective analysis of cEEG (≥ 6 months; recorded between
63 January 2004 and May 2018) collected with an FDA-approved implanted device in 175 adults
64 with drug-resistant focal epilepsy followed at 35 centers across the USA. In distinct
65 development and validation cohorts, subjects had ≥ 20 electrographic and disabling clinical
66 (self-reported) seizures, respectively. In all subjects, the device stored interictal epileptiform
67 activity (IEA) that revealed cycles of abnormal brain activity. Point process statistical models
68 trained on initial portions of each subject's data generated forecasts of seizure probability that
69 were tested on subsequent unseen data and evaluated against surrogate time-series. The
70 primary outcome was the percentage of subjects with forecasts showing improvement over
71 chance (IoC).

72

73 **Findings**

74 Models incorporating information about IEA cycles generated daily seizure forecasts with IoC in
75 15/18 (83%) subjects and 104/157 (66%) subjects in the development and validation cohorts,
76 respectively. In many subjects, the forecasting horizon could be extended up to three days.
77 Hourly forecasts, possible only in the development cohort, showed IoC in 18/18 (100%)
78 subjects.

79

80 **Interpretation**

81 Seizure probability can be reliably forecasted days in advance using data from an approved
82 device. For adults with focal epilepsy, personalized risk-stratification over days is
83 unprecedented and may enable novel seizure prevention strategies. This study paves the way
84 for prospective clinical trials that will establish how people with epilepsy may benefit from long-
85 horizon seizure forecasting.

86

87 **Funding**

88 None.

89 Introduction

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Epilepsy is defined by the seemingly random occurrence of spontaneous seizures. Although seizures are typically brief events that cumulatively amount to a small fraction of time, their unpredictability necessitates standing treatments and causes significant disability.¹ People with epilepsy are plagued by constant uncertainty, and the looming threat of seizures has implications for personal safety, independence, and psychological well-being. Reliable methods to anticipate seizures would mark a paradigm shift in clinical epilepsy, mitigating this uncertainty and enabling time-varying, risk-based seizure prevention strategies.

Despite decades of progress in the field of seizure prediction, such methods remain elusive.² The landmark NeuroVista trial³ demonstrated feasibility of a cEEG-based advisory system that warned of seizures minutes in advance. Subsequent analyses⁴⁻¹⁰ of data from this trial yielded numerous transformative insights that propelled the field for years. However, limitations of these pioneering efforts include the relatively small size of the trial—ten subjects participated in the seizure advisory phase—and the fact that the implanted device used is no longer available.

In the decade since the NeuroVista trial, cEEG from another device (RNS[®] System), one that is FDA-approved and increasingly used in clinical care for epilepsy,¹¹ revealed pervasive daily (circadian^{12,13}) and multi-day (multidien¹³) cycles of interictal epileptiform activity (IEA) that are biomarkers of seizure risk.¹³ With these long-timescale biomarkers,¹⁴⁻¹⁶ interest has recently shifted to probabilistic approaches to seizure forecasting,^{5,17,18} akin to weather forecasting, which leverage prior knowledge about cyclical patterns of seizure risk to estimate seizure probability over future time horizons. Since most prior work in the field has sought to identify seizure precursors in the minutes preceding seizure onset,^{2,8} an unresolved question concerns whether periods of heightened seizure risk (pro-ictal states¹⁸) can be anticipated over longer horizons. We hypothesized that seizure probability is determined by alignment of cyclical influences at multiple timescales as well as the temporal distribution of recent seizures.^{4,9,10,18} Models that incorporate these factors to generate seizure risk forecasts will ultimately require validation in large, prospective clinical trials. Imminent feasibility of such trials hinges on evaluating how generalizable and valuable the approach may be on existing cEEG data, using a probabilistic framework that accounts for the fact that seizures may not occur every time risk is accurately forecasted to be high.

Here, we address these questions in a feasibility study aimed at developing and validating statistical models to forecast the individual risk for electrographic and self-reported seizures based on temporal features extracted from up to ten years of cEEG data. The primary study outcome was the percentage of subjects for whom forecasting models demonstrated Improvement over Chance (IoC) at different forecasting horizons. Secondary outcomes involved quantifying model performance using statistical methods suitable for probabilistic forecasts.

129 **Methods**

130

131 **Study design and participants**

132 This feasibility study involved development of seizure forecasting models in a ‘development
133 cohort’ of 18 subjects who were implanted with the RNS® System (NeuroPace, Inc., Mountain
134 View, CA, USA) for clinical indications and followed at two centers (University of California, San
135 Francisco, and California Pacific Medical Center, USA). Forecasting models were subsequently
136 validated by including cEEG data and self-reported seizures obtained from a ‘validation cohort’
137 of 157 participants in the nine-year long-term treatment trial (LTT) of the RNS System^{11,19} that
138 took place between January 2004 and May 2018 across 34 centers in the USA (appendix, pp 10–
139 11; ClinicalTrials.gov identifiers: NCT00079781, NCT00264810, and NCT00572195). All involved
140 centers obtained authorization from their institutional review board to recruit adults with
141 medically-refractory focal epilepsy in the original trials and for subsequent data analysis.
142 Existing cEEG data and seizure logs were screened for eligibility: > 6 months of continuous
143 hourly IEA count data without large gaps and ≥ 20 electrographic or self-reported seizures but <
144 50% days with seizures, as the utility of forecasting in individuals with very frequent seizures is
145 likely low.³ All 175 included subjects provided written informed consent for analysis of their
146 data.

147

148 **Procedure**

149 The RNS System utilizes customizable algorithms to detect pathological brain activity, as
150 previously detailed.¹³ For each subject, IEA time-series from two RNS System detectors
151 (appendix, pp 10–16) were selected for periods of continuous data with stable detection
152 settings > 6 months. For all subjects, the first few months of cEEG (median [range] 222 d [28–
153 362 d]) after device implantation were discarded to account for time needed by clinicians to
154 optimize detection parameters.

155

156 Self-reported seizures are the current gold-standard for clinical trials in epilepsy, but
157 electrographic seizures evident on cEEG are more objective and obviate subjects’ reporting
158 biases.²⁰ Therefore, we examined two types of seizures drawn from distinct, non-overlapping
159 cohorts of subjects: (1) Timestamps of electrographic seizures from cEEG in the development
160 cohort (N=18), identified through detections of prolonged epileptiform activity exceeding a
161 clinically pre-specified duration, typically 15–40s. For each subject and each period of stable
162 detection settings, a Board-certified epileptologist (V.R.R.) verified visually that ≥90% of these
163 detections corresponded to electrographic seizures in stored electrocorticograms, as described
164 in detail previously¹³; (2) Diaries of self-reported seizures in the validation cohort (N=157),
165 recorded by participants in the LTT as number of seizures (‘simple motor’, ‘simple other’,
166 ‘complex partial’, and ‘generalized tonic-clonic’) per calendar day. According to the 2017
167 International League Against Epilepsy classification, we considered ‘complex partial’ and
168 ‘generalized tonic-clonic’ as the disabling ‘seizures with impaired awareness’ studied here and

169 excluded subjects without disabling seizures. As subjects did not report the time of day for their
170 seizures, these data could only be used for daily and not for hourly forecasts.

171

172 **Statistical analysis**

173 Forecasting models: To forecast seizure probabilities—continuous values between 0 (no risk of
174 seizure occurrence) and 1 (seizure occurrence is certain)—we used past IEA, occurrence times
175 of past seizures, and cyclical variables (hereafter, collectively referred to as ‘temporal features’)
176 as inputs for point process generalized linear models (PP-GLMs). Models were estimated on
177 training data and evaluated on chronologically subsequent test data. PP-GLMs are established
178 tools in neuroscience research^{21,22} that provide a flexible statistical framework to evaluate the
179 association between sequences of event (seizure) times represented as binary (or count) time-
180 series and temporal features upon which event probability may depend. Hourly IEA time-series
181 were available for electrographic and self-reported seizure cohorts, allowing determination of
182 circadian and multidien cycles of epileptic brain activity in all subjects (N=175).¹³ We trained PP-
183 GLMs with a log-link function and a conditionally Poisson distribution²² to output the probability
184 of a seizure as a function of these cycles and other temporal features (appendix, pp 9–10) from
185 subject-specific datasets comprising the shorter of 480 d or 60% of the subject’s total data. To
186 prevent inflation of our performance metrics (see below) through the well-known phenomenon
187 of seizure clustering, we defined ‘seizure-days’ or ‘seizure-hours’ as binary events regardless of
188 the seizure count and used these as training labels. The large amount of previously unseen
189 testing data (Individually: minimum of 40% of data, >800 d in most subjects and up to 8 y; In
190 total: 73% of data with 211,005 d) ensured that the models were not overfit for a small number
191 of seizures and enabled assessment of forecasting performance in a probabilistic framework.

192

193 Outcomes: Subject-specific forecast performance was quantified on held-out test datasets (i.e.
194 index test) containing unseen seizures (i.e. reference standard: days or hours with self-reported
195 or electrographic seizures) using two complementary metrics that are fully described in the
196 appendix (pp 1–9): (i) for various seizure warning threshold probabilities, the area under the
197 curve (AUC) of sensitivity (proportion of all seizures captured during warning) vs. corrected
198 proportion of time in warning;²³ (ii) Brier skill score (BSS), adapted from meteorology,^{5,17} which
199 evaluates performance in relation to a naïve predictor (here, a randomly shuffled forecast).

200

201 Based on these metrics, the primary outcome was Improvement over Chance (IoC), a binary
202 outcome defined at the individual level through comparison of the original AUC to chance-level
203 AUC, calculated from forecasts issued on surrogate data (see Statistical significance).^{2,5,8,23} In
204 addition, secondary outcomes involved quantifying individual forecast performance. We
205 calculated the median AUC across subjects with IoC (and the entire cohort) to evaluate
206 discrimination, the goal of a deterministic forecast (do forecasts differ when their
207 corresponding observations differ? see appendix, pp 1–9). AUC depends heavily on forecast
208 horizon and pro-ictal state duration, and AUC is less than 1 even for a reliable forecast
209 (appendix, p 8). This motivated the additional use of the BSS, which assesses model resolution
210 (are different forecasts associated with different outcomes?) and calibration (how close are

211 forecasted probabilities to observed probabilities?), the goals of a probabilistic forecast
212 (appendix, pp 1–9). Reliability diagrams⁵ were used to compare observed and forecasted
213 seizure probabilities.

214
215 Post-hoc analyses: To characterize individualized forecasts in terms of time-varying risk, we
216 defined pro-ictal states as periods of time with forecasted probability above the individual
217 expected seizure probability (appendix, pp 1–9). Based on these adjusted values, we report the
218 average duration of pro-ictal states and the relative risk for seizures in pro-ictal as compared to
219 low-risk states. We evaluated the overlap between forecasted probabilities and observed
220 seizures as a function of circadian and multidien cycle phases and AUC as a function of the
221 strength of seizure cycles, quantified as the phase-locking value (appendix, p 24).¹³

222
223 Sensitivity analyses: Robustness of our results was assessed by systematically varying the
224 amount of training data and the retraining interval (appendix, pp 21–23).

225
226 Statistical significance: To determine individual chance-level AUCs, 200 surrogates were
227 generated for each temporal feature: (1) for the recent seizure, circadian, and weekly
228 distribution models, by randomly shuffling the seizure time-series under the null hypothesis
229 that the seizure process is memoryless (i.e. events are independent of one another); (2) for the
230 IEA-based features, by randomizing phases of underlying cycles, under the null hypothesis that
231 seizure timing does not depend on trends in IEA.^{24,25} Significance was assessed with a false
232 discovery rate (FDR) at $\alpha = 0.05$ across all subjects to correct for multiple testing. As a
233 supplementary statistical analysis, significance of AUC was assessed by comparing the number
234 of seizures correctly identified by the model and by chance for a given fraction of time under
235 warning (appendix, p 28).^{23,26} Analyses were performed with MATLAB R2019a, R 3.4.4, and
236 Python 3.7.4.

237 238 **Role of funding source**

239 This study received no targeted funding. All authors had full access to data and had
240 responsibility for the decision to submit for publication.

241 242 **Data sharing**

243 Deidentified individual data in the form of IEA counts and electrographic seizures from the 18
244 subjects in the development cohort, as well as code created and used for this paper, will be
245 freely available at **#DOI will be made available upon acceptance#** as of July 1, 2021 for at least
246 20 years. A short explanation of the data is also provided. Original study protocols, statistical
247 analysis plan, and informed consent forms are not available for this retrospective study. Data
248 for the validation (self-reported seizure) cohort is property of NeuroPace, Inc. and is not
249 available.

250
251

252 Results

253
254 We collected retrospective cEEG data from two cohorts of subjects implanted with the RNS
255 System (Fig. 1a, mean duration per subject 1484 d, range 227–3502 d). Between January 1,
256 2018 and October 1, 2019, we screened 72 and 256 subjects, and we included 18 and 157
257 subjects in distinct cohorts for forecasting model development and validation, respectively
258 (flow diagram). The development cohort comprised 10 subjects whose cEEG data we previously
259 published¹³ but here extended to include two years of subsequent recordings, plus 8 new
260 subjects. The validation cohort comprised a subset of participants in the nine-year RNS System
261 Long-term Treatment Trial (LTT)¹⁹, from which only limited cEEG data has been published¹².
262 cEEG data (Fig. 1b) from this cohort was used to validate forecasting models, which were then
263 tested against the published dataset of self-reported seizures from the LTT¹⁹. Baseline
264 characteristics for the two cohorts were similar, with median age 38 [IQR 32–51] and 35 [IQR
265 25–43], and 44% (8/18) and 47% (74/157) females, respectively, with a preponderance of
266 multifocal and mesio-temporal epilepsies (Table 1).

267 In both cohorts, forecasting models were individually estimated on the first portion of
268 each subject’s data, the ‘training datasets’, and tested on non-overlapping individual ‘testing
269 datasets’ containing a total of 767 electrographic (median 19% [IQR 13–29] days with seizures)
270 and 27,658 self-reported seizures (median 9% [IQR 5–16] days with seizures) that were
271 previously unseen (see Methods). To forecast seizure probability with horizons of hours to days,
272 models incorporated past IEA, occurrence times of past seizures, and cyclical variables as inputs
273 (hereafter, ‘temporal features;’ Fig. 1c, Table 2). Individual subjects had excellent
274 correspondence between forecasts and seizures (Fig. 1d–h).

275 As a primary outcome, and for each temporal feature, we determined which subjects
276 might benefit from forecasting with our models by calculating improvement over chance (IoC:
277 AUC relative to chance-level, Table 2). Daily forecasts incorporating information only about
278 recent seizures, weekly seizure distribution, or recent IEA produced IoC less often than models
279 using information from multidien IEA cycles, for which IoC was observed in 15/18 (83%) and
280 104/157 (66%) subjects for electrographic and self-reported seizures, respectively (Fig. 2a; Table
281 2). With multidien IEA cycles alone, the forecast horizon could be extended up to three days
282 while maintaining IoC in 2/18 (11%) and 61/157 (39%) subjects for electrographic and self-
283 reported seizures, respectively (Fig. 2b).

284 As secondary outcomes, we quantified forecast performance for subjects with IoC using
285 two complementary metrics, each addressing a distinct question (appendix, pp 1–9): (i) Area
286 under the curve (AUC, sensitivity vs. corrected time in warning)—How valuable is a forecast
287 given the amount of time spent in warning?, and (ii) Brier skill score^{5,17}—How well does the
288 forecast perform relative to a reference strategy (BSS = 1 for perfect forecast; BSS = 0 for no
289 improvement over a random predictor)? Median AUC was 0.74 [IQR 0.70–0.79] and 0.70 [IQR
290 0.65–0.75], and median BSS was 0.23 [IQR 0.18–0.30] and 0.13 [IQR 0.05–0.20] in the
291 development (electrographic seizures) and validation (self-reported seizures) cohorts,
292 respectively (Fig. 2a, c; all median values in Table 2; appendix, pp 17–18). A reliability diagram⁵

293 showed that resolution (Fig. 2d, highest bin average is below 1) and calibration were good, but
294 not perfect, with forecasted probabilities above 25% being overconfident (i.e. below the
295 diagonal line of perfect calibration, Fig. 2d).

296 As a post-hoc analysis, we characterized the durations of forecasted pro-ictal states, i.e.
297 the tendency for daily forecasts to remain high over consecutive days (Fig. 1f). To allow for
298 comparison across subjects, we averaged peak-aligned forecasts centered within subjects
299 around expected seizure probability (appendix, pp 1–9). This enabled visualization of pro-ictal
300 states as contiguous periods of heightened seizure probability lasting 3–9 d and aligning well
301 with the distributions of observed electrographic and self-reported seizures (Fig. 3). Average
302 relative risk (RR) for self-reported and electrographic seizures occurring during forecasted pro-
303 ictal versus low-risk states was 9.4 [95% CI 4.5–14.9] and 3.7 [95% CI 2.8–4.7] across subjects
304 with IoC. Model performance also correlated with phase-locking values between seizures and
305 multidien IEA cycles¹³ (Pearson $r=0.6547\pm 2.7\times 10^{-3}$, Wald test, $p<0.0001$; appendix, p 24),
306 suggesting that the most forecastable individuals can be identified in advance.

307 To further characterize performance of daily forecasts, we carried out sensitivity
308 analyses to inclusion criteria (appendix, pp 19–20) and to training conditions. In both cohorts,
309 longer training duration and iterative retraining (appendix, p 23), improved model performance
310 and the calibration of output forecast probability (Fig. 2d; appendix, pp 21–22).

311 Forecasting days-long pro-ictal states over long horizons may not be ideal for all
312 patients,^{27,28} so we asked whether our approach allows refinement of forecasts to shorter
313 horizons. Equivalent outcomes were obtained for hourly forecasting, which was only possible
314 for electrographic seizures, as subjects in the validation cohort reported seizure days but not
315 hours. Multivariate models incorporating instantaneous phases of circadian and multidien
316 cycles and the recent circadian distribution of seizures⁵ yielded the best-performing hourly
317 forecasts of electrographic seizures (Fig. 4a, c; appendix, p 25), and IoC was observed in 18/18
318 subjects (100%; Table 2; appendix, pp 25–26). The forecasting horizon could be extended up to
319 14 h while maintaining IoC in 8/18 subjects (44%; Fig. 4b). Across subjects, highest forecasted
320 seizure probabilities occurred when critical phases of multidien and circadian cycles aligned (Fig.
321 4d).

322

323

324 Discussion

325

326 Here, we forecasted electrographic seizures and self-reported seizures—a gold standard metric
327 for clinical trials in epilepsy—up to three days in advance. To our knowledge, this represents an
328 unprecedented horizon for personalized seizure risk-stratification. Daily forecasts were above
329 chance in the majority of the 175 adults with focal epilepsy involved in this feasibility study
330 (15/18 and 104/157 in development and validation cohorts, respectively). In all subjects for
331 whom it was possible (18/18), forecasts of electrographic seizures achieved finer temporal
332 resolution on the scale of hours. Included subjects were treated with an implanted
333 neurostimulation device and may not be representative of all people with epilepsy, though
334 diverse focal epilepsies were represented in our cohorts, and seizure cycles are independent of
335 brain stimulation.^{13,15}

336 To date, there has been only one prospective trial (NeuroVista³) of a seizure advisory
337 system, which provided short-term (minutes) warnings of imminent seizures demonstrating
338 above-chance accuracy in 9 out of 15 (60%) enrolled subjects (10 of these subjects completed a
339 4-month testing period). Subsequent analyses on the same dataset showed that even the most
340 difficult cases were predictable to some extent through crowd-sourced computational efforts.⁶⁻⁸
341 In comparison, our feasibility study involved ten times more subjects, testing and validating a
342 single computational approach for periods up to 10 years, and forecast horizons several orders
343 of magnitude longer (hours to days).

344 To evaluate forecasting model performance rigorously, we comprehensively report
345 measurements of risk, discrimination, resolution, and calibration (explained in appendix, pp 1–
346 9). During forecasted pro-ictal states, the average RR of occurrence of electrographic and self-
347 reported seizures was 9.4 and 3.7, respectively, placing cycles of epileptic brain activity among
348 the strongest predictors of seizures discovered to date. While RR is a well-established metric in
349 medicine, it is limited to the evaluation of probabilistic forecasts at a single threshold value,
350 whereas the BSS circumvents this limitation, offering a refined interpretation of forecast
351 performance as a continuum (appendix, pp 1–9). A recent study in nine subjects employed
352 probabilistic methods similar to ours within a circadian framework and yielded BSS ranging
353 0.02–0.2 at a forecast horizon of one minute.⁵ In comparison, our study provided well-
354 calibrated forecasts, as illustrated in a reliability diagram (Fig. 2b), and median BSS of 0.23 [IQR
355 0.18–0.30] (electrographic seizures) and 0.13 [IQR 0.05–0.20] (self-reported seizures). Another
356 key distinction of our work is that daily forecasts of higher seizure probabilities were aggregated
357 over days-long pro-ictal states (Fig. 3), providing smooth forecasts rather than flickering alerts
358 based on real-time detection of evanescent seizure precursors. This may improve the
359 interpretability of forecasts for people with epilepsy.³

360 This study has limitations. Implanted devices are associated with surgical risks and may
361 not be suitable for all people with epilepsy who desire seizure forecasts, motivating
362 development of minimally-invasive methods to monitor seizure risk biomarkers.^{1,4} Cycles of IEA
363 may be more tractable than biomarkers requiring high sampling rate intracranial EEG,²⁹ opening
364 the possibility that certain novel methods, like sub-scalp EEG,³⁰ could be viable for forecasting.

365 Our models did not incorporate common seizure triggers, such as medication non-compliance,
366 which could account for some apparent 'false negatives.' Self-reported seizure data was drawn
367 from a large, prospective, nine-year clinical trial^{11,19}—arguably the most well-curated clinical
368 seizure dataset of this chronicity—but inaccuracy of seizure self-reports^{3,20} and small gaps in the
369 data could have led to under-estimation of model performance. Finally, to dissect the potential
370 contribution of different temporal features, this feasibility study focused on explicit statistical
371 models that are computationally efficient, modest in their training requirements, and
372 incorporated cycles of IEA using an accurate but non-causal estimation of the instantaneous
373 phases. Thus, conclusions should be regarded as hypothesis-generating rather than clinical
374 evidence.⁸

375 In summary, our results corroborate an emerging view that seizures are not entirely
376 random events.⁸ Given the large sample size, these results validate and powerfully extend our
377 previous findings based solely on electrographic seizures,¹³ and they suggest the generalizability
378 of using multiscale cyclical biomarkers in epileptic brain activity to forecast clinically-relevant
379 seizures over long horizons. Moreover, our study indicates that seizure forecasting is feasible
380 with existing neurotechnology in widespread clinical use (~3,000 patients currently implanted in
381 the U.S.) and need not await novel industrial developments. Future prospective clinical trials
382 should assess directly the ways in which people with epilepsy benefit from replacing constant
383 uncertainty about seizures with “measured uncertainty” (forecasted risk) at different horizons,
384 which has not been established by this or prior studies. To that end, we propose a nested
385 approach to personalized seizure forecasting: (1) patient-specific multidien cycles reveal pro-
386 ictal states days in advance; (2) circadian IEA cycles and peak seizure times reveal hours of high
387 risk;⁵ and (3) real-time detections of seizure precursors² provide imminent seizure warnings
388 conditioned on prior probability from (1) and (2). Future work will also involve miniaturization
389 of devices, integration of cEEG with multimodal physiological data,¹ optimization of forecasting
390 models, and elucidation of mechanisms underlying cycles in epilepsy.

391

392

393 **Legends**

394

	Development cohort	Validation cohort
N	18	157
Age in years (median [IQR])	38 [32-51]	35 [25-43]
Percent females	44% (8/18)	47% (74/157)
Percent males	56% (10/18)	53% (83/157)
Seizure studied	Electrographic seizures	Self-reported disabling seizures
Bilateral focus	50% (9/18)	46% (73/157)
Left-sided focus	33% (6/18)	39% (62/157)
Right-sided focus	17% (3/18)	14% (22/157)
Mesiotemporal lobe epilepsy	83% (15/18)	64% (101/157)
Frontal lobe epilepsy	0% (0/18)	9% (14/157)
Multilobar epilepsy	6% (1/18)	12% (19/157)
Other neocortical epilepsy	11% (2/18)	15% (23/157)
Percentage of days with seizures in training datasets (median [IQR])	25% [17-29]	15% [10-25]
Percentage of days with seizures in testing datasets (median [IQR])	19% [13-29]	9% [5-16]

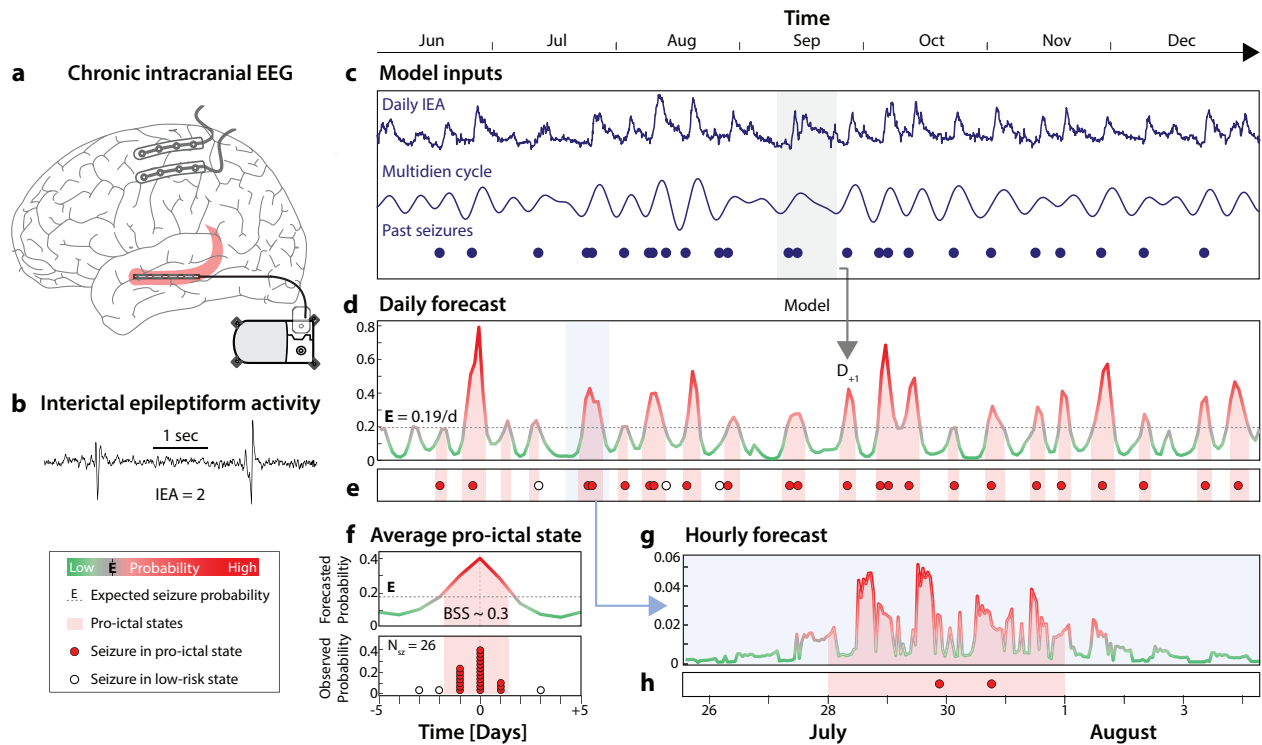
395 **Table 1.** Demographics and seizure characteristics of all subjects in the development and
 396 validation cohorts.

397

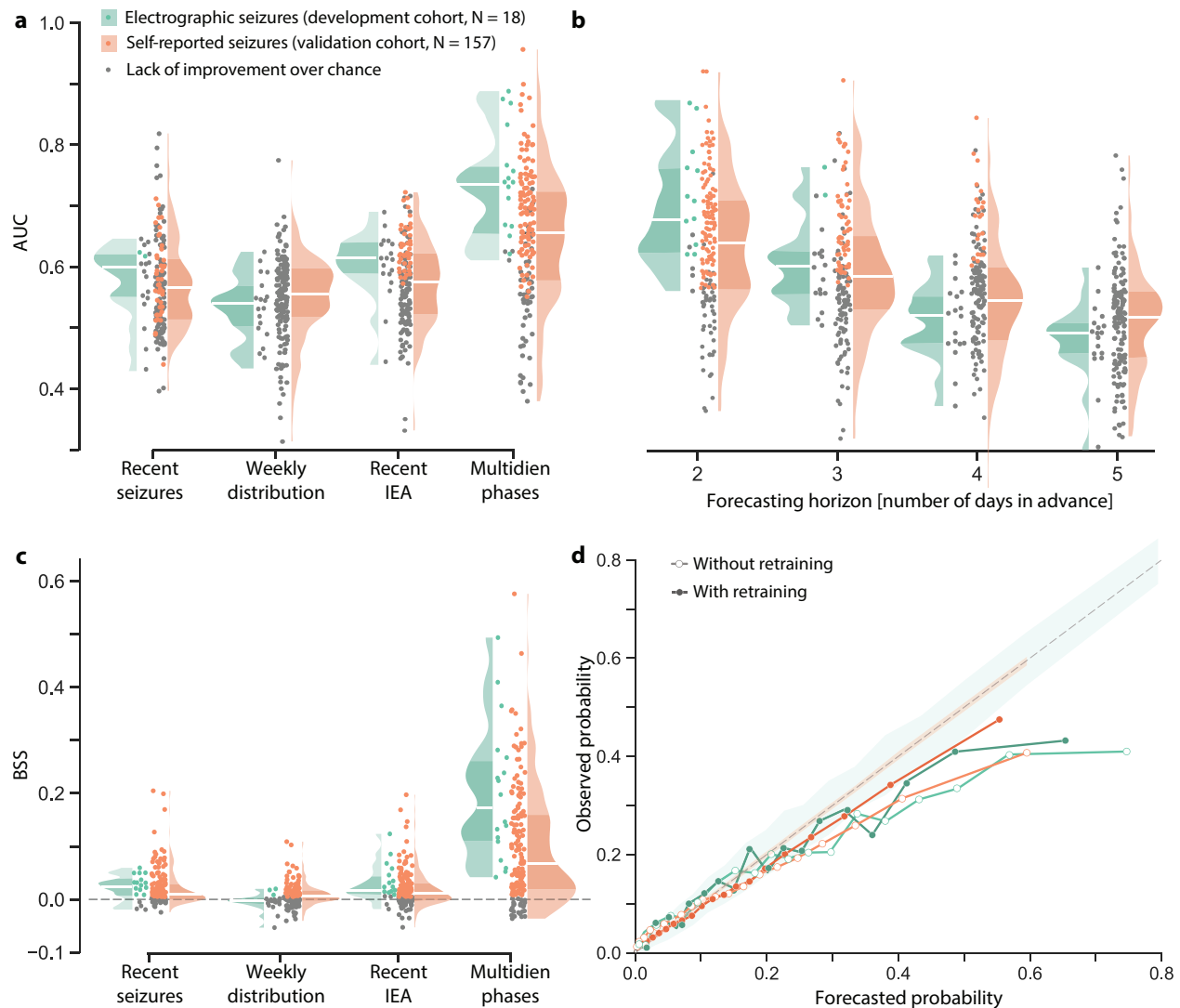
Horizon		Forecasts								
		Daily						Hourly		
Cohort		Development (N=18)			Validation (N=157)			Development (N=18)		
Reference standard		Electrographic seizures			Self-reported disabling seizures			Electrographic Seizures		
Study outcome		1°	2°		1°	2°		1°	2°	
Metric		IoC	AUC	BSS	IoC	AUC	BSS	IoC	AUC	BSS
Temporal features	Recent seizures	2/18 (11%)	0.62 (0.60)	0.06 (0.03)	43/157 (27%)	0.58 (0.57)	0.012 (0.009)	6/18 (33%)	0.57 (0.52)	0.002 (0.00)
	Recent IEA	0/18 (0%)	NA (0.61)	NA (0.02)	51/157 (32%)	0.62 (0.58)	0.04 (0.01)	5/18 (28%)	0.64 (0.60)	0.008 (0.006)
	Circadian IEA phases	NA	NA	NA	NA	NA	NA	8/18 (44%)	0.65 (0.62)	0.01 (0.01)
	Circadian seizure distribution	NA	NA	NA	NA	NA	NA	11/18 (61%)	0.62 (0.59)	0.008 (0.002)
	Weekly seizure distribution	0/18 (0%)	NA (0.54)	NA (0.00)	0/157 (0%)	NA (0.56)	NA (0.004)	NA	NA	NA
	Multidien phases	15/18 (83%)	0.74 (0.73)	0.23 (0.17)	103/157 (66%)	0.70 (0.66)	0.13 (0.07)	15/18 (83%)	0.70 (0.70)	0.024 (0.018)
	Multivariate	NA	NA	NA	NA	NA	NA	18/18 (100%)	0.75 (0.75)	0.036 (0.035)

399 **Table 2. Primary and secondary study outcomes.** Percentage of subjects with Improvement
400 over Chance (IoC) for different temporal features, where IoC was obtained by comparing the
401 area under the curve (AUC) of the original data with the AUC of 200 surrogate time-series with
402 alpha < 0.05 adjusted for false-discovery rate correction. Data are median AUC and median
403 Brier skill score (BSS) among subjects with IoC (entire cohort). 1°: primary, 2°: secondary.

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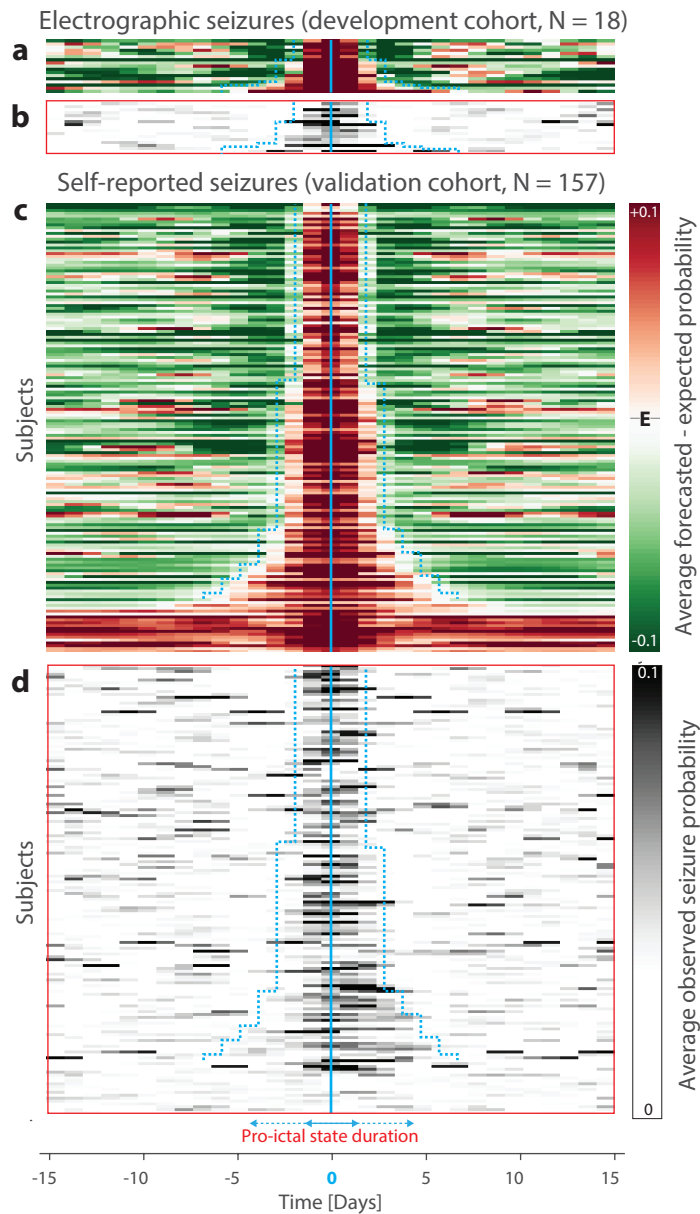


407
 408 **Figure 1. Individual seizure risk forecasting in one subject.** (a) Responsive Neurostimulation
 409 (RNS[®]) System, comprising a cranially-implanted neurostimulator connected to two four-
 410 contact intracranial depth leads (shown, for example, in hippocampus, red) and/or cortical strip
 411 leads (shown unconnected) that provide chronic electroencephalography (cEEG). (b) From these
 412 recordings, the RNS System provides hourly counts of detections of interictal epileptiform
 413 activity (IEA) and electrographic seizures (not shown). (c-e) Entire test dataset from one subject
 414 (S7) showing input temporal features, output daily forecasts, and observed seizures. (c) Time-
 415 series of IEA averaged over one calendar day ('daily IEA'), underlying multidien cycle, and
 416 electrographic seizures that serve as some of the input temporal features for the forecasting
 417 model. (d) Daily forecast of seizure probability (gradient-colored lines) at 24-hour horizon (D_{+1})
 418 generated by a model (grey arrow) trained on ten months of data (not shown) and run on seven
 419 months of held-out test data (shown here) using input variables from c. Higher forecasted
 420 probabilities (red) form days-long pro-ictal states (red shadow) during which daily probability of
 421 seizures is continuously above the expected probability, defined as the long-term average daily
 422 seizure frequency calculated over months of training data ('E', here 0.19 seizures per day). (e)
 423 Seizures observed during and outside of pro-ictal states over these seven months. (f) Average
 424 pro-ictal state illustrated by peak-aligned average probability forecasts (top) and corresponding
 425 temporal distribution of seizures (bottom, shown as stacked individual events and percentage
 426 of total count on y-axis). (g) Hourly forecasts of seizure probability based on hourly IEA and its
 427 circadian cycle (not shown) refining pro-ictal states into hours of relatively higher and lower
 428 seizure risk. BSS: Brier skill score. (h) Seizures observed over this period of nine days.
 429



430
 431 **Figure 2. Performance of daily forecasts of electrographic and self-reported seizures.** (a)
 432 Distributions of univariate daily forecast performance (at 24-h horizon) quantified as the area
 433 under the curve (AUC) across subjects. When models incorporated multidien phase information,
 434 AUC showed improvement over chance (IoC) for 83% and 66% of subjects (color dots, $p < 0.05$) in
 435 the development cohort (with recorded electrographic seizures) and the validation cohort (with
 436 self-reported seizures), respectively. Shaded areas in these and subsequent violin plots show
 437 kernel density estimates to highlight the shape of the distribution of the entire cohort; darker
 438 shading is the interquartile range and horizontal white line is the median. (b) AUC as a function
 439 of forecasting horizon longer than 24-hour using multidien phase as the input variable, to be
 440 compared to forecast at 24-hour horizon in a. (c) As in (a), daily forecasts based on multidien
 441 phases of IEA yielded both higher AUC and Brier skill score (BSS) than other models. The BSS
 442 represents improvement (skill, color dots) of mean squared forecast error (Brier score) relative
 443 to a reference randomly shuffled forecast; BSS range is $-\infty$ to 1, with 0 being no skill relative to
 444 reference forecast and 1 being a perfect forecast. (d) Reliability diagram showing observed

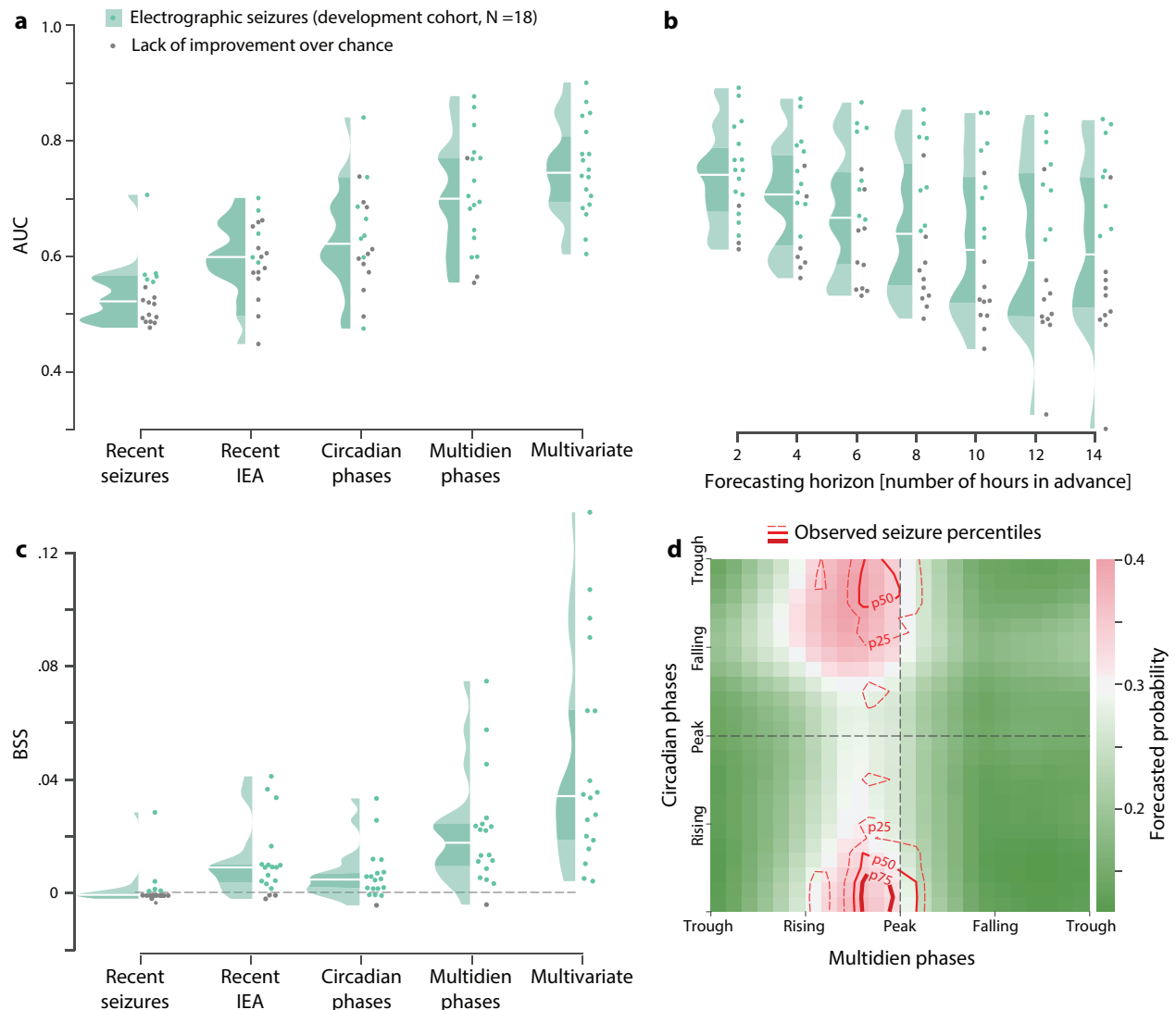
445 seizure probability vs. binned forecasted probabilities of electrographic seizures (green, N=18
446 subjects) and self-reported seizures (orange, N=157 subjects). Empirical curves for a set of
447 forecasts generated by models before (empty dots) and after (filled dots) re-training after every
448 seizure are compared to the dashed diagonal line of perfect calibration (shading indicates 95%
449 confidence intervals (CI)).
450



452

453 **Figure 3. Pro-ictal states.** (a) Peak-aligned normalized average forecast probabilities for all
 454 subjects in the electrographic seizures (development) cohort (N=18, rows, ranked by width of
 455 pro-ictal state) reveal days-long periods of seizure probability higher than the expected seizure
 456 probability (E). (b) Distributions of observed seizure probabilities averaged in the same way align
 457 well with periods of high risk. (c) and (d) show data analogous to (a) and (b) from the self-reported
 458 seizures (validation) cohort (N=157). Cyan boundaries depict estimated durations of pro-ictal
 459 states, which range from three to five days in the majority of subjects and more than seven days
 460 in a minority of subjects. Most subjects whose forecasts did not show IoC reside at the bottom,
 461 outside of the cyan boundaries.

462



463
 464 **Figure 4. Hourly forecasts of electrographic seizures.** Hourly forecasts were not possible for
 465 self-reported seizures because time resolution of these data was one day. **(a)** Distributions of
 466 univariate and multivariate hourly forecast performance (at 1-h horizon) quantified as the AUC
 467 across subjects. Multivariate models incorporated information from circadian and multidien
 468 phases of IEA, as well as the circadian distribution of seizures, yielding AUC with IoC in 18 out of
 469 18 (100%) subjects (color dots, $p < 0.05$). **(b)** AUC as a function of forecasting horizon hours in
 470 advance of seizures. **(c)** As in (a), multivariate models yielded both higher AUC and BSS than
 471 univariate models. **(d)** Phase-space map across 18 subjects showing alignment of critical phases
 472 of circadian and multidien cycles with observed seizures (contours represent percentiles),
 473 coinciding with times of highest forecasted seizure probability.

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477 **Online content**

478 Any methods, additional references, reporting summaries, source data, statements of data
479 availability, and associated accession codes are available in the online version of the paper.

480

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490

491 **Author contributions**

492 M.O.B., T.P., V.R.R., and W.T. designed the study. V.R.R. and D.K.S collected the data of the
493 development cohort. T.K.T. provided the data of the validation cohort. V.R.R., T.K.T., and M.O.B.
494 accessed, selected, and verified the data. T.P., W.T., M.G.L., and M.O.B. performed the analysis.
495 T.P., M.O.B., and V.R.R. wrote the manuscript, which all authors edited.

496

497 **Competing interests**

498 M.O.B reports personal fees from Wyss Center for neurotechnology as part-time employee,
499 grants from Wyss Center for neurotechnology, outside the submitted work; In addition, Dr.
500 Baud has a pending patent under the Patent Cooperation Treaty (#62665486). V.R.R reports
501 personal fees from NeuroPace, Inc., outside the submitted work. T.K.T. is an employee of
502 NeuroPace, Inc. and receives salary and stock options as compensation. T.P., W.T., M.G.L., and
503 D.K.-S. have nothing to disclose.

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